



**KAPITAŁ LUDZKI**  
NARODOWA STRATEGIA SPÓJNOŚCI

**UNIA EUROPEJSKA**  
EUROPEJSKI  
FUNDUSZ SPOŁECZNY



## **„Medical Imaging”**

**Prezentacja multimedialna współfinansowana przez  
Unię Europejską w ramach  
Europejskiego Funduszu Społecznego w projekcie pt.  
*„Innowacyjna dydaktyka bez ograniczeń - zintegrowany  
rozwój Politechniki Łódzkiej - zarządzanie Uczelnią,  
nowoczesna oferta edukacyjna i wzmacniania zdolności  
do zatrudniania osób niepełnosprawnych”***



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# Quality of medical images

## Lecture overview:

Definition of image quality

Main factors influencing the quality

- unsharpness
- contrast
- noise
- distortions and artifacts

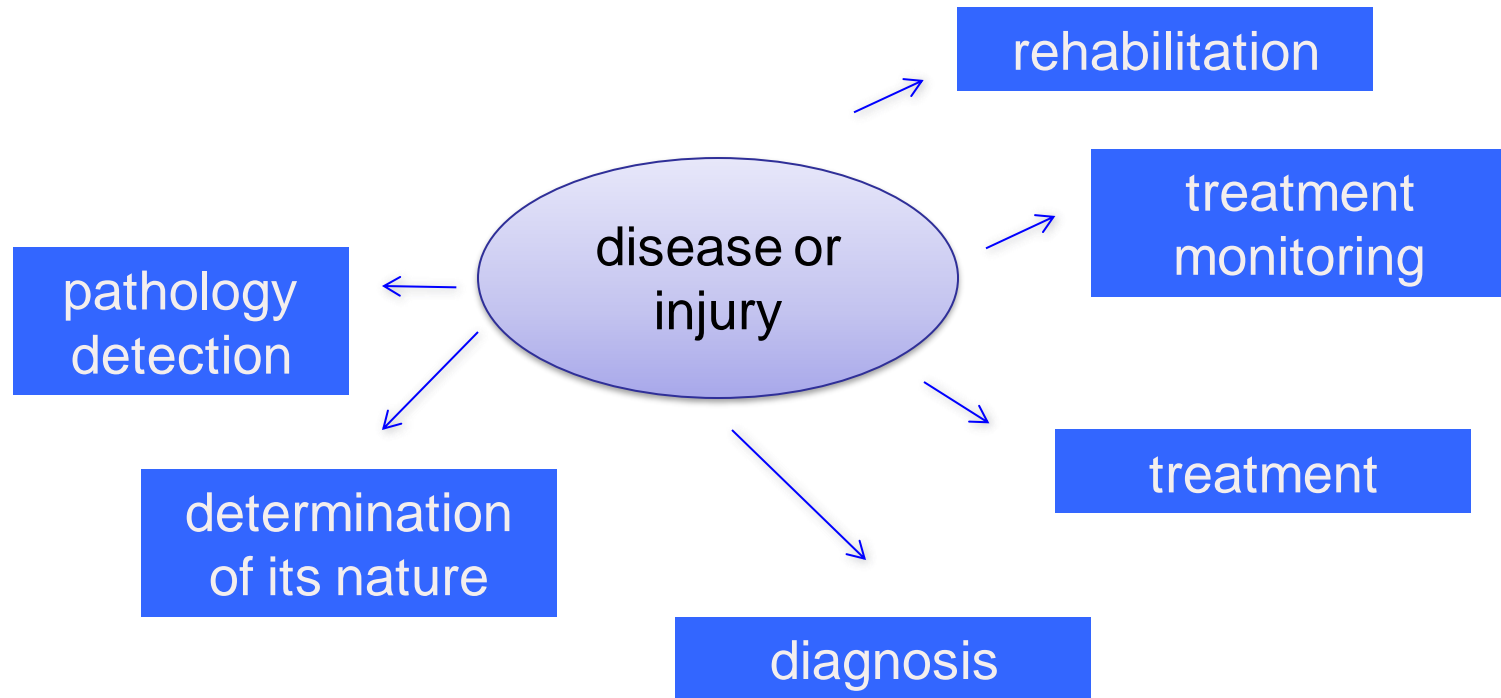
Quantitative assessment of the image quality





# Image quality

The purpose of medical imaging:

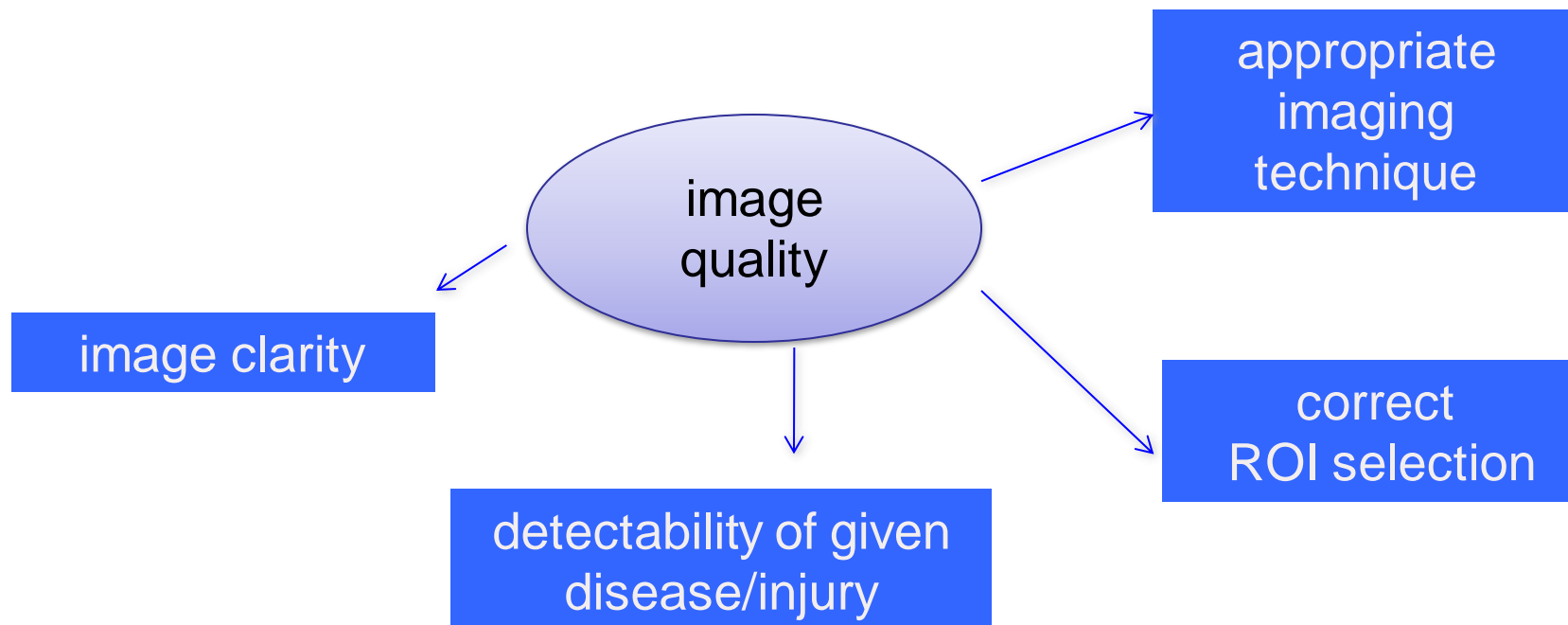


The degree to which the image achieves its purpose is considered as “image quality”





# Image quality

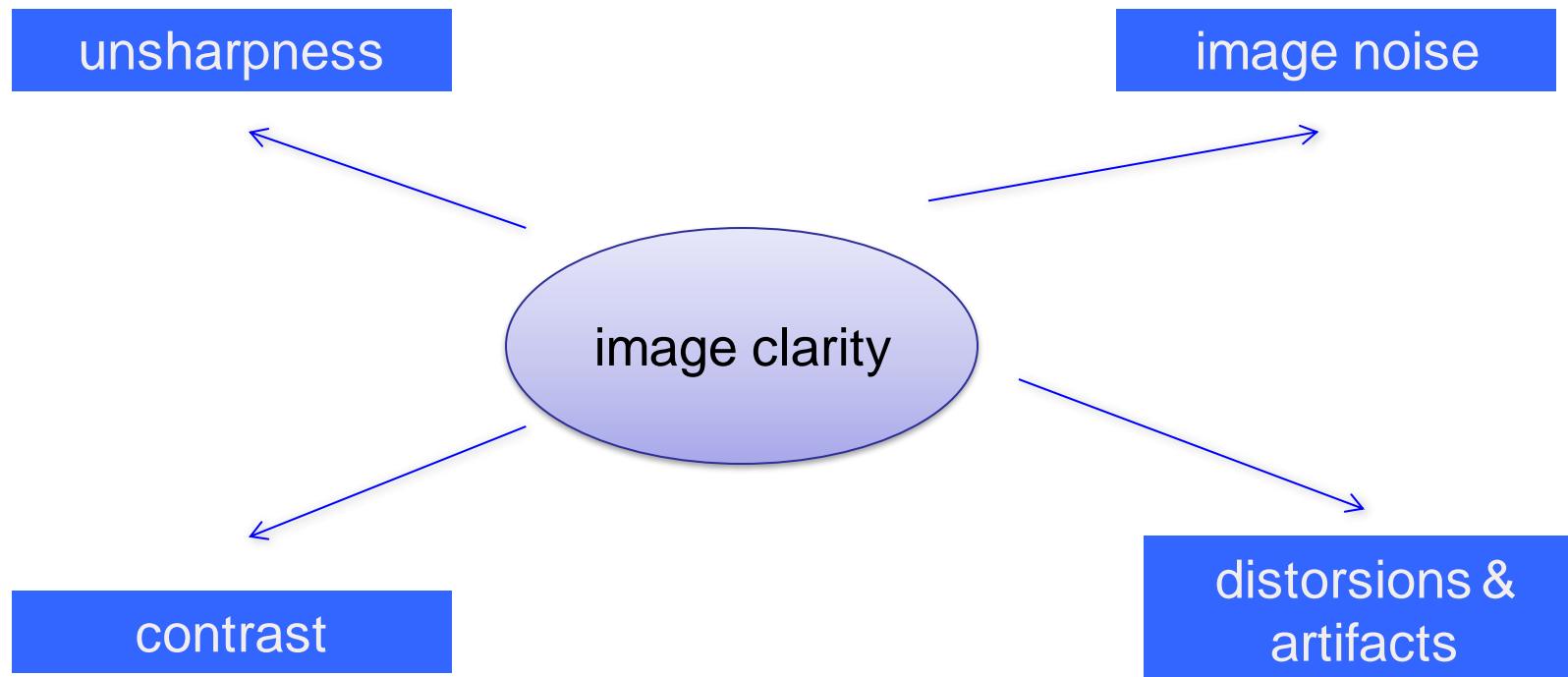


A measure of how well information of interest (about the anatomy, physiology, functional capacity) is displayed in an image



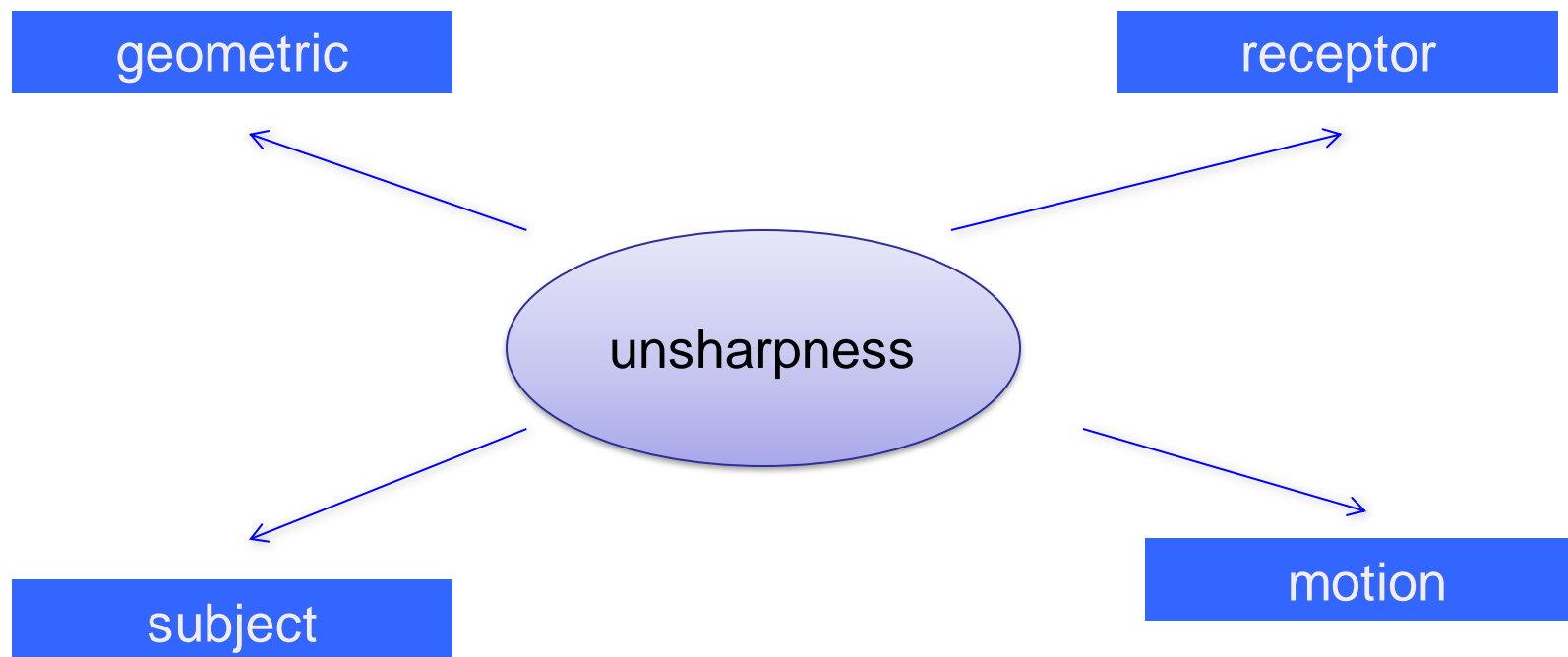


# Image clarity





# Unsharpness

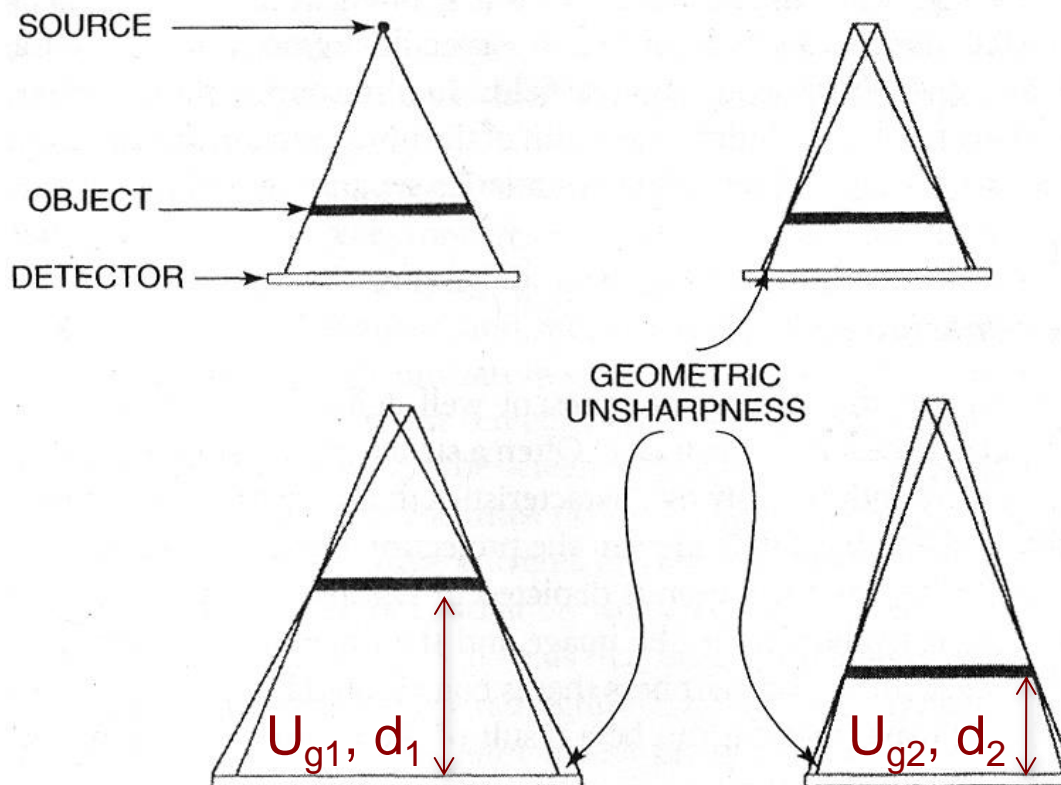


$$U = \sqrt{U_g + U_s + U_m + U_r}$$





# Geometric unsharpness

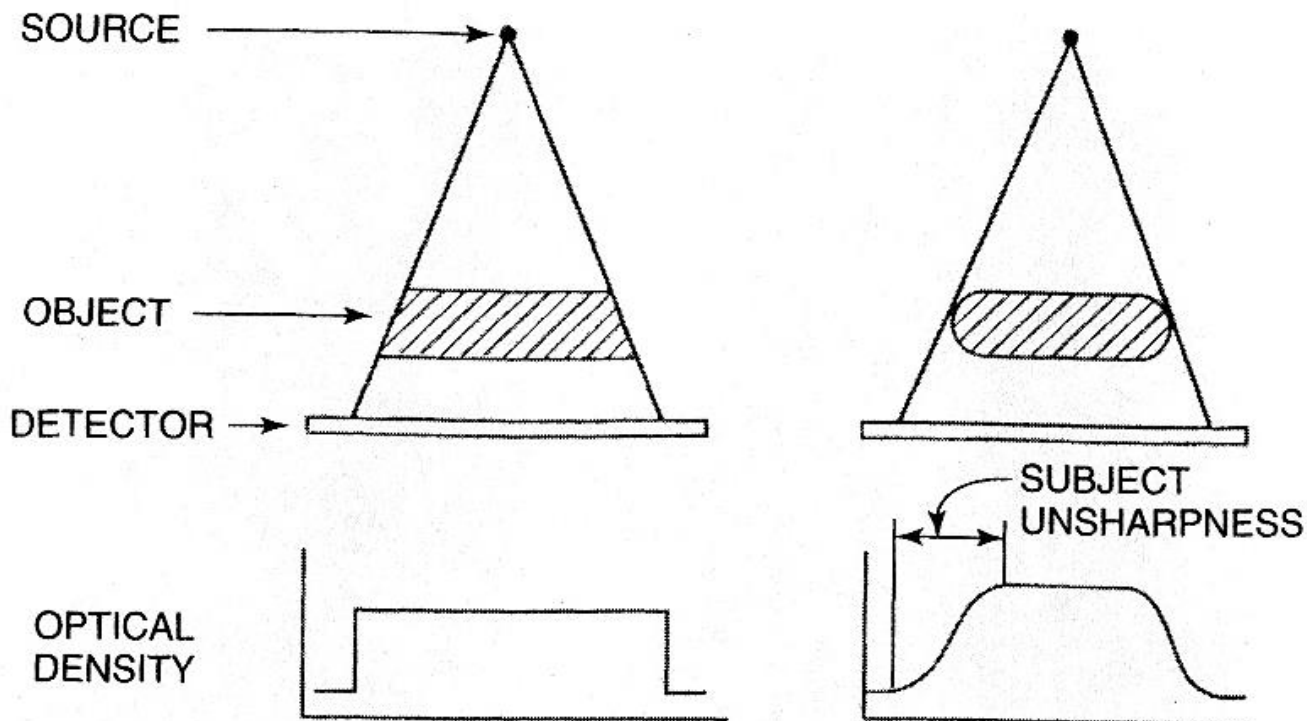


$$d_1 > d_2 \Rightarrow U_{g1} > U_{g2}$$





# Subject unsharpness







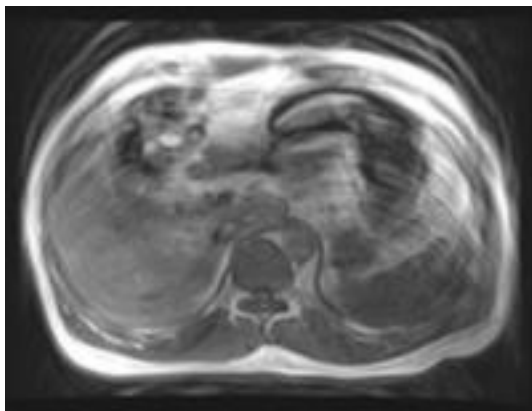
# Motion unsharpness

Anatomic structure	Speed [mm/s]
Head	1-2
Upper abdomen	20-40
Lower abdomen	15-30
Lungs	70-100 (150-200)
Heart muscle	60-90 (100-130)

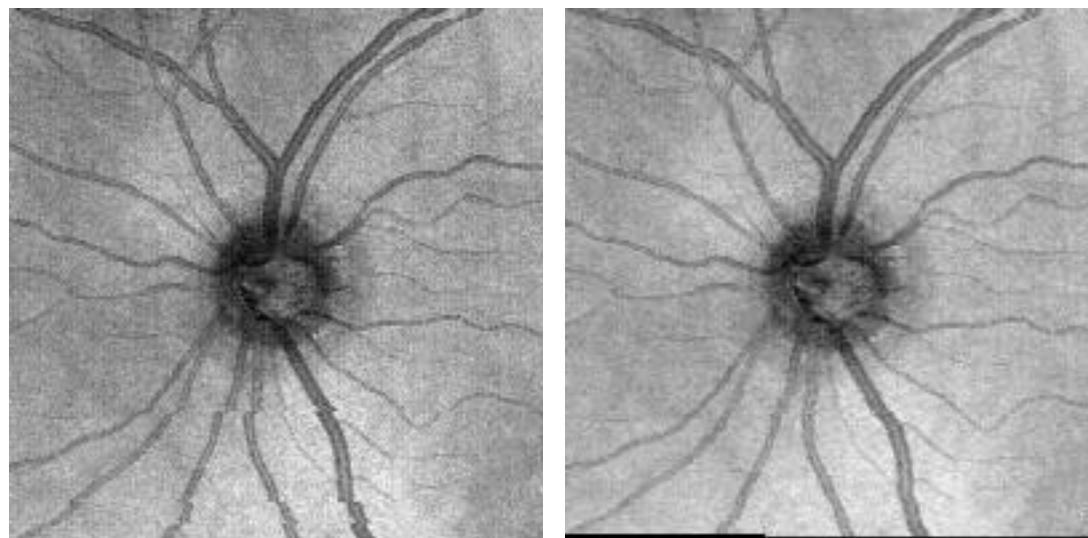




# Motion artifacts



MR example



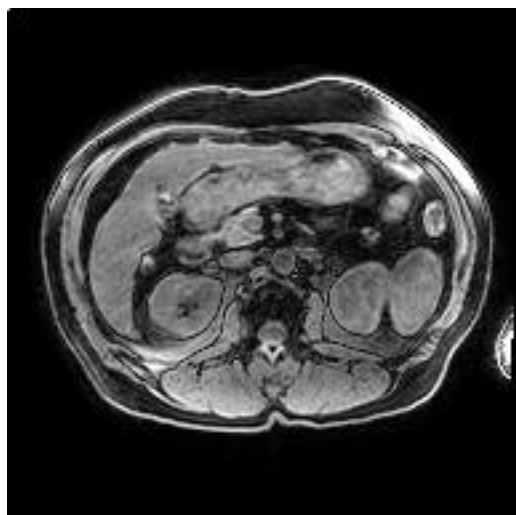
Optical Coherence Tomography example



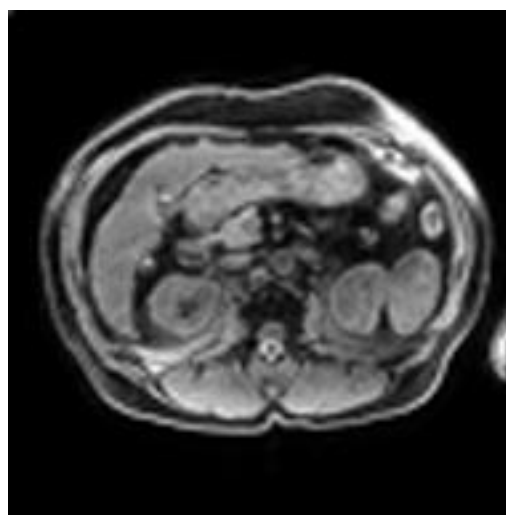


# Receptor unsharpness

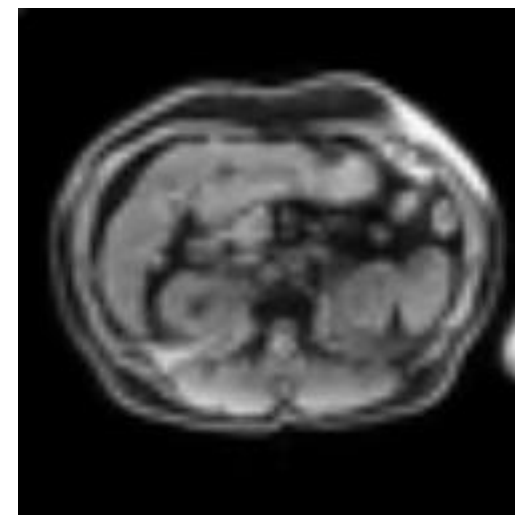
Introduced by the process, which converts the data acquired by given visualisation technique into an image



matrix: 192x192  
FOV: 400x400 mm



matrix: 96x96  
FOV: 400x400 mm

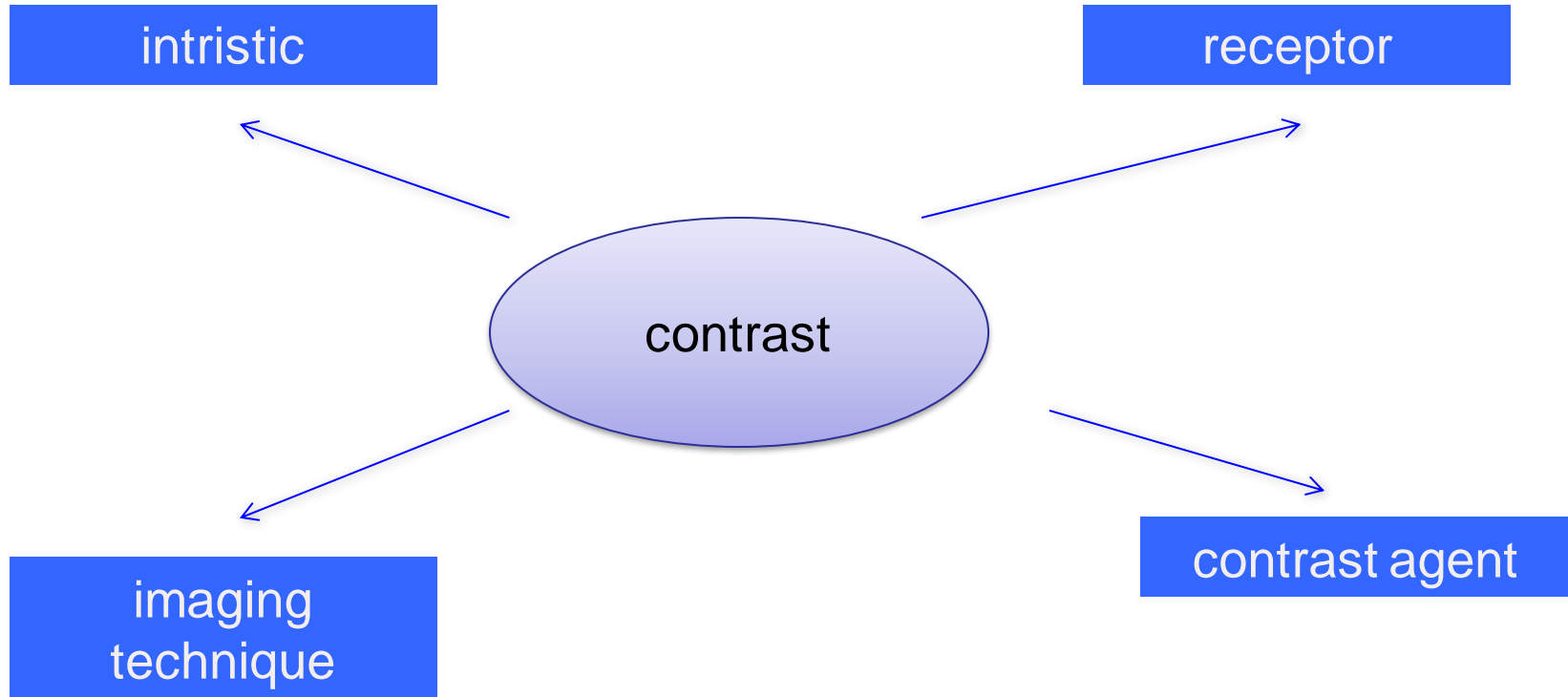


matrix: 64x64  
FOV: 400x400 mm





# Image contrast



Contrast describes the ability of distinguishing of subtle features (details) in the object



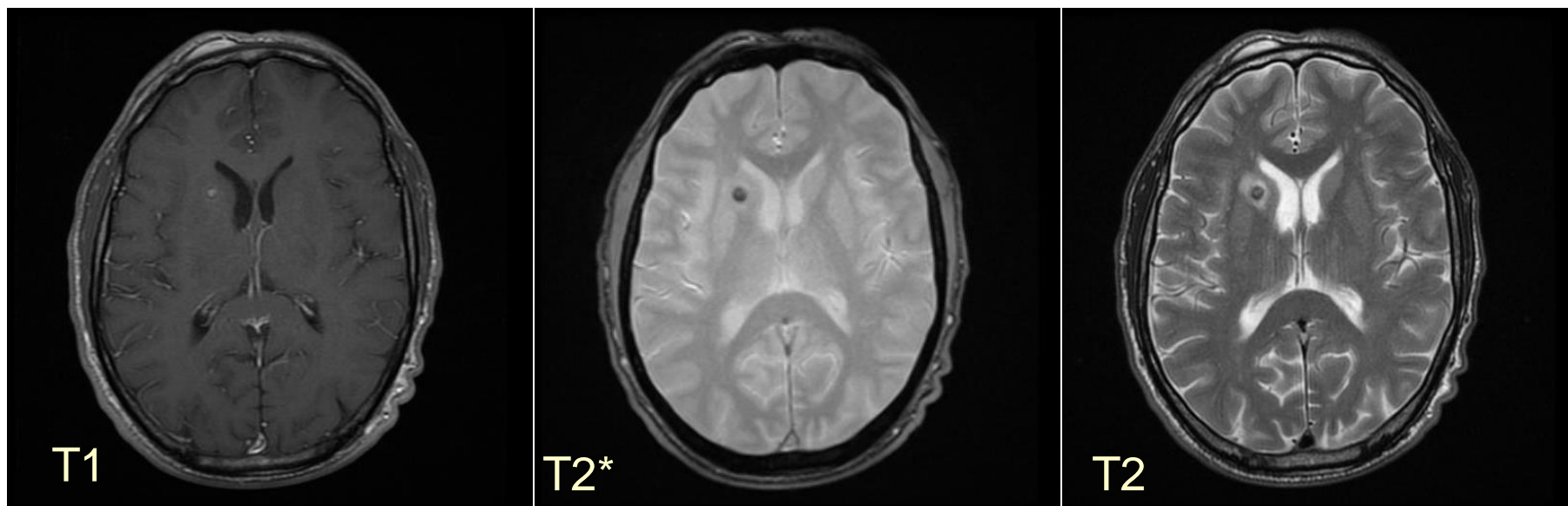
# Intrinsic (subject, object, patient) contrast

<b>Radiography</b>	<b>Nuclear medicine</b>	<b>Ultrasound</b>	<b>Computed Tomography</b>	<b>Magnetic Resonance</b>
Physical density	Activity	Velocity	Physical density	Proton density
Atomic number	Distribution	Acoustic impedance	Electron density	Relaxation times
Absorption	Concentration	A/R/S	Absorption	RF waves

Represents the difference in physical composition of visualised structures



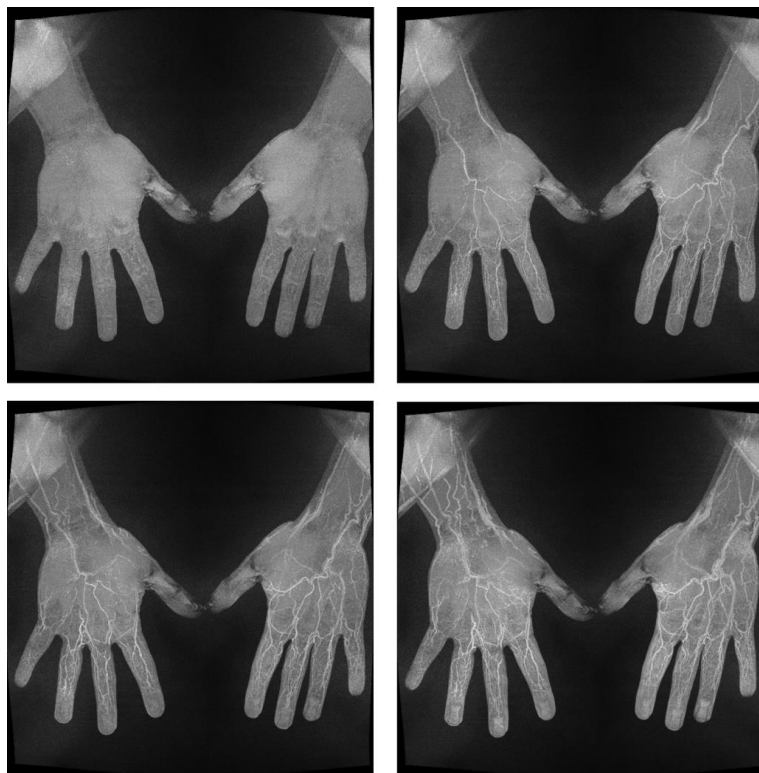
# Imaging technique



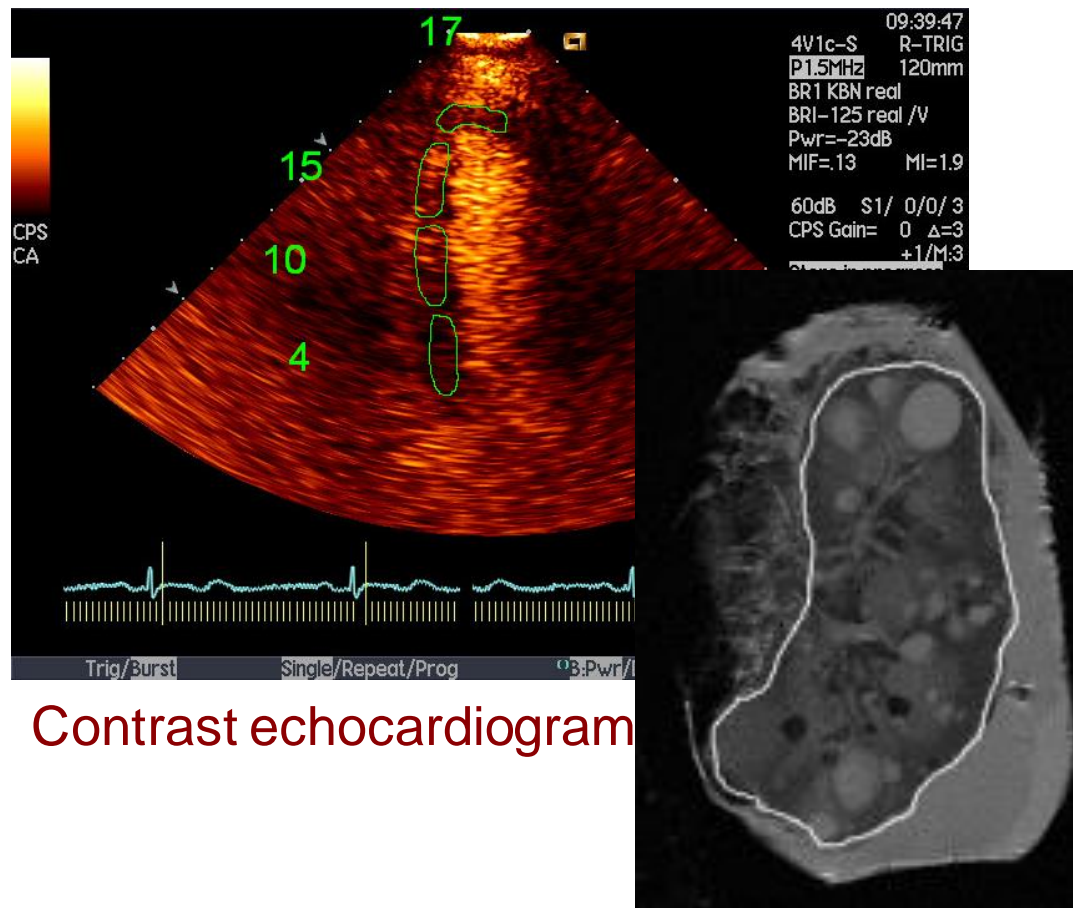
Different MR acquisition protocols (sequences)



# Contrast agents



MR angiography  
(Vasovist)



Contrast echocardiogram

Left kidney (MR, gadolinium)



# Receptor contrast

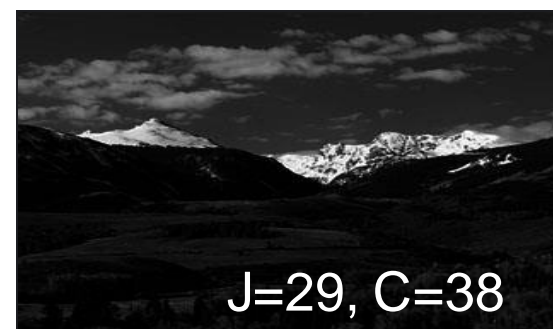
Depends on properties of image converting/displaying devices

Brightness

$$B = \frac{1}{MN} \sum_{i=1}^M \sum_{j=1}^N f(i, j)$$

Contrast

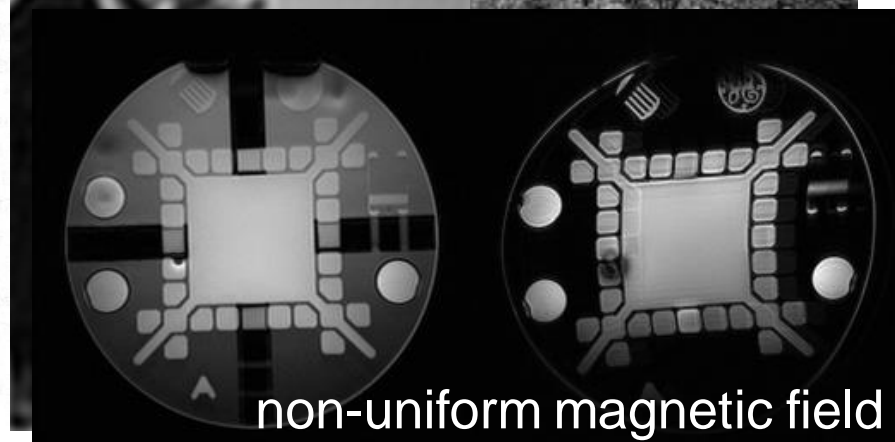
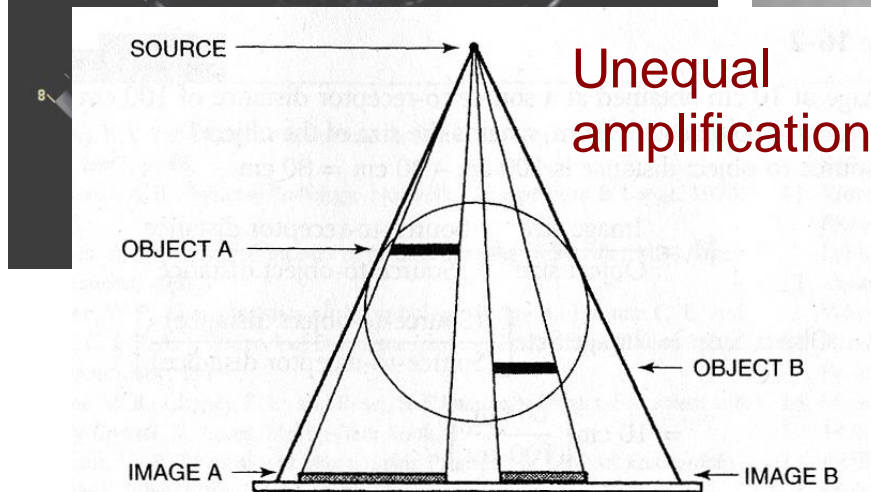
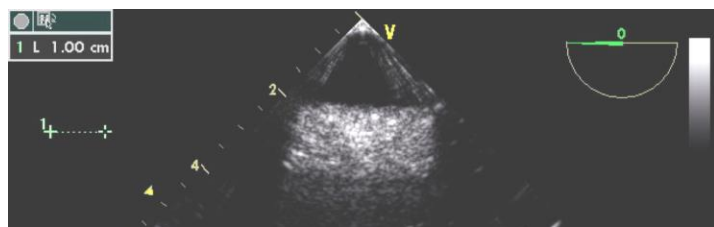
$$C = \sqrt{\frac{1}{MN} \sum_{i=1}^M \sum_{j=1}^N [f(i, j) - J]^2}$$



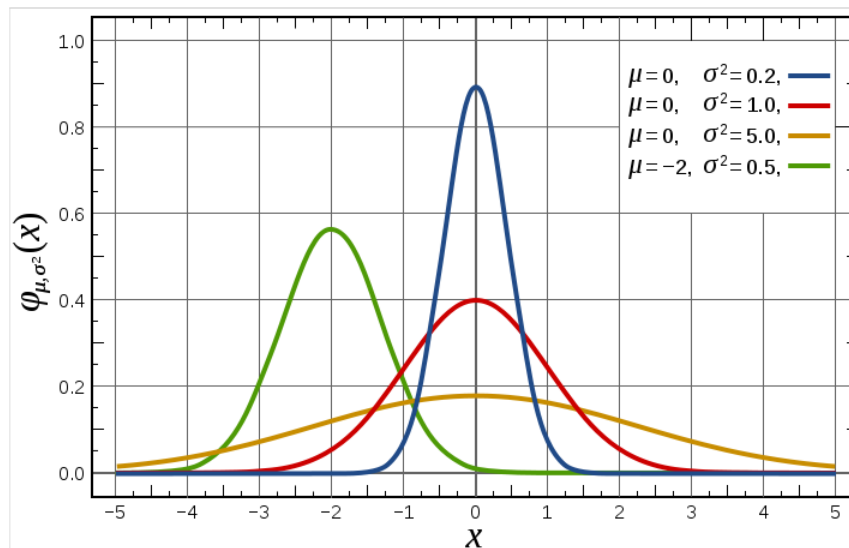
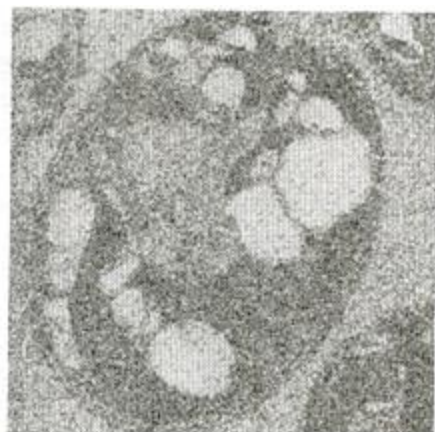


# Distorsions & artifacts

Caused e.g. by image formation system (optical), unequal amplification (radiography), non-uniform magnetic field (MR), multiple echos (ultrasound), ...

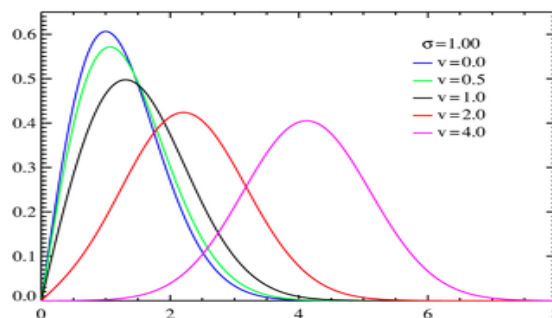
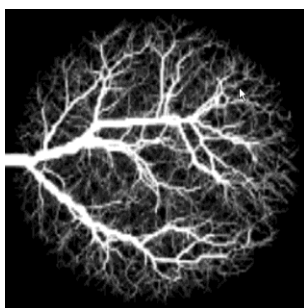


# Image noise



Gaussian noise

$$n_g(x) = \frac{1}{\sqrt{2ps^2}} e^{-\frac{(x-m)^2}{2s^2}}$$



$$n_r(x) = \frac{x}{S} e^{-\frac{(x^2 - n^2)}{2s^2}} I_0\left(\frac{xn}{s}\right)$$

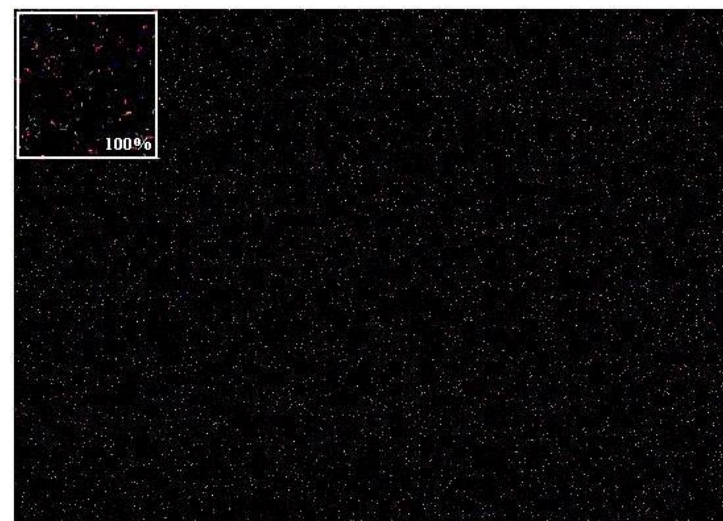
Rician noise (MR)



# Image noise



Pulse noise  
(random distribution of maximal & minimal intensities)



Pulse noise in CCD matrix

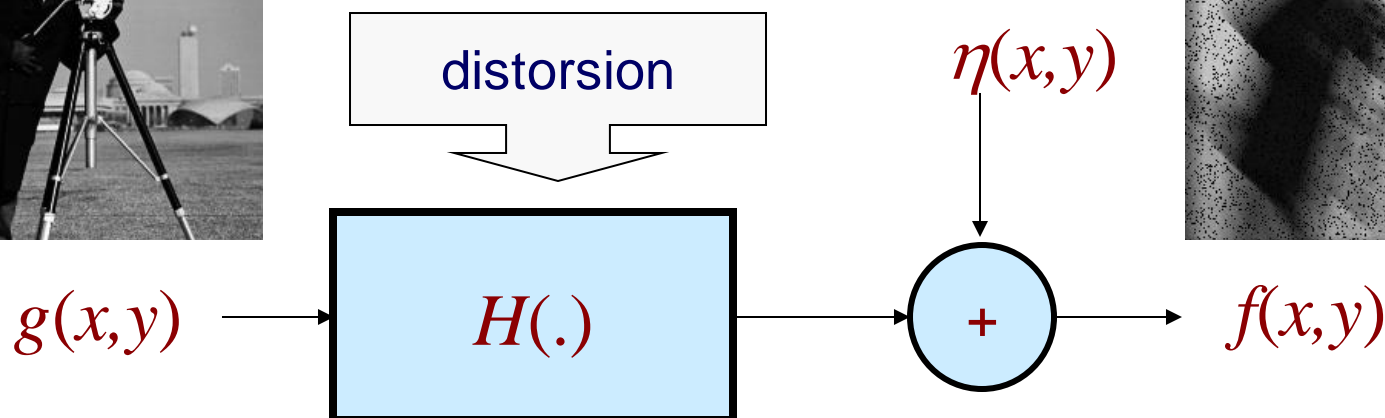


# Image degradation model

## Source image



## Degraded image



$$f(x,y) = H[g(x,y)] + \eta(x,y)$$

# Signal to noise ratio

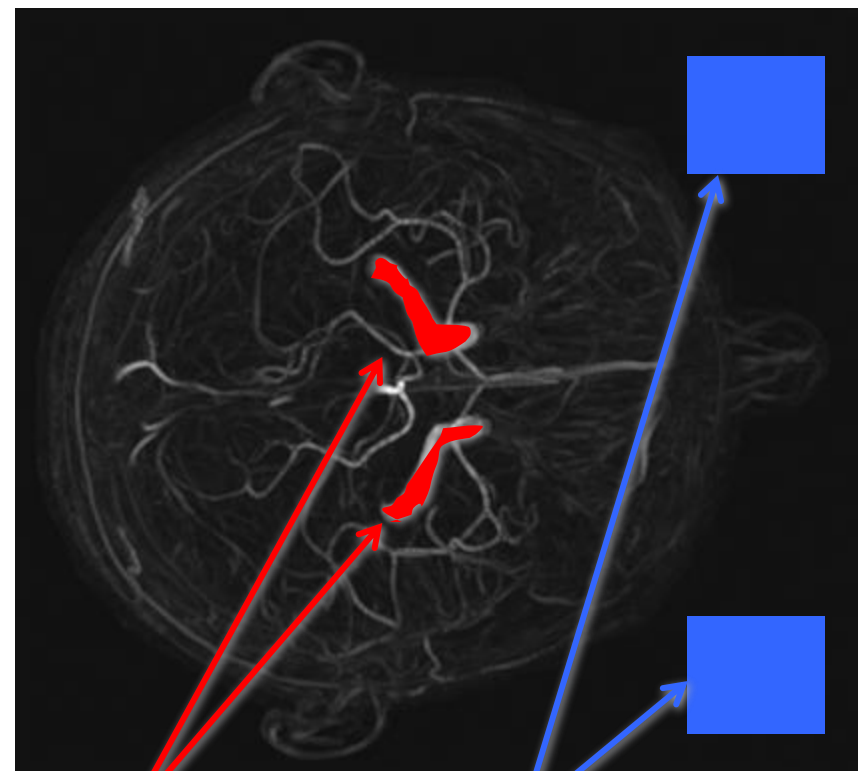
Signal-to-noise ratio (SNR or S/N) is a quantitative measure of image quality, it estimates how much an image has been corrupted by noise.

$$SNR = \frac{P(f)}{P(n)}$$

$$SNR_{dB} = 10 \log_{10} \frac{P(f)}{P(n)}$$

SNR in practice:

$$SNR = \frac{m_{signal}}{S_{noise}^2}$$



ROIs for  
estimation  
of  $\mu_{signal}$

ROIs for  
estimation  
of  $\sigma_{noise}$



# Inverse filter

$$G(u, v) = H(u, v) \cdot F(u, v) + N(u, v)$$

$$\hat{F}(u, v) = \frac{1}{H(u, v)} \cdot G(u, v) = F(u, v) + \frac{1}{H(u, v)} \cdot N(u, v)$$

Inverse filter

Estimation of inverse filter characteristic may cause problems for frequencies when  $H(u, v) \approx 0$





# Wiener filter

$$G(u, v) = H(u, v) \cdot F(u, v) + N(u, v)$$

$$\hat{F}(u, v) = \frac{1}{H(u, v)} \times \frac{|H(u, v)|^2}{|H(u, v)|^2 + \frac{S_n(u, v)}{S_f(u, v)}} \times G(u, v)$$

- $S_f(u, v)$ ,  $S_n(u, v)$  – power spectrum densities for source image and distorted image, respectively
- It is assumed that  $K$  is estimated as  $(\text{SNR})^{-1}$
- for small frequencies or  $K \rightarrow 0$  Wiener filter corresponds to inverse filter
- for  $K \rightarrow \infty$  Wiener filter approaches to low-pass filter

# Wiener filter – application example



source  
image



distortion  
(shift)



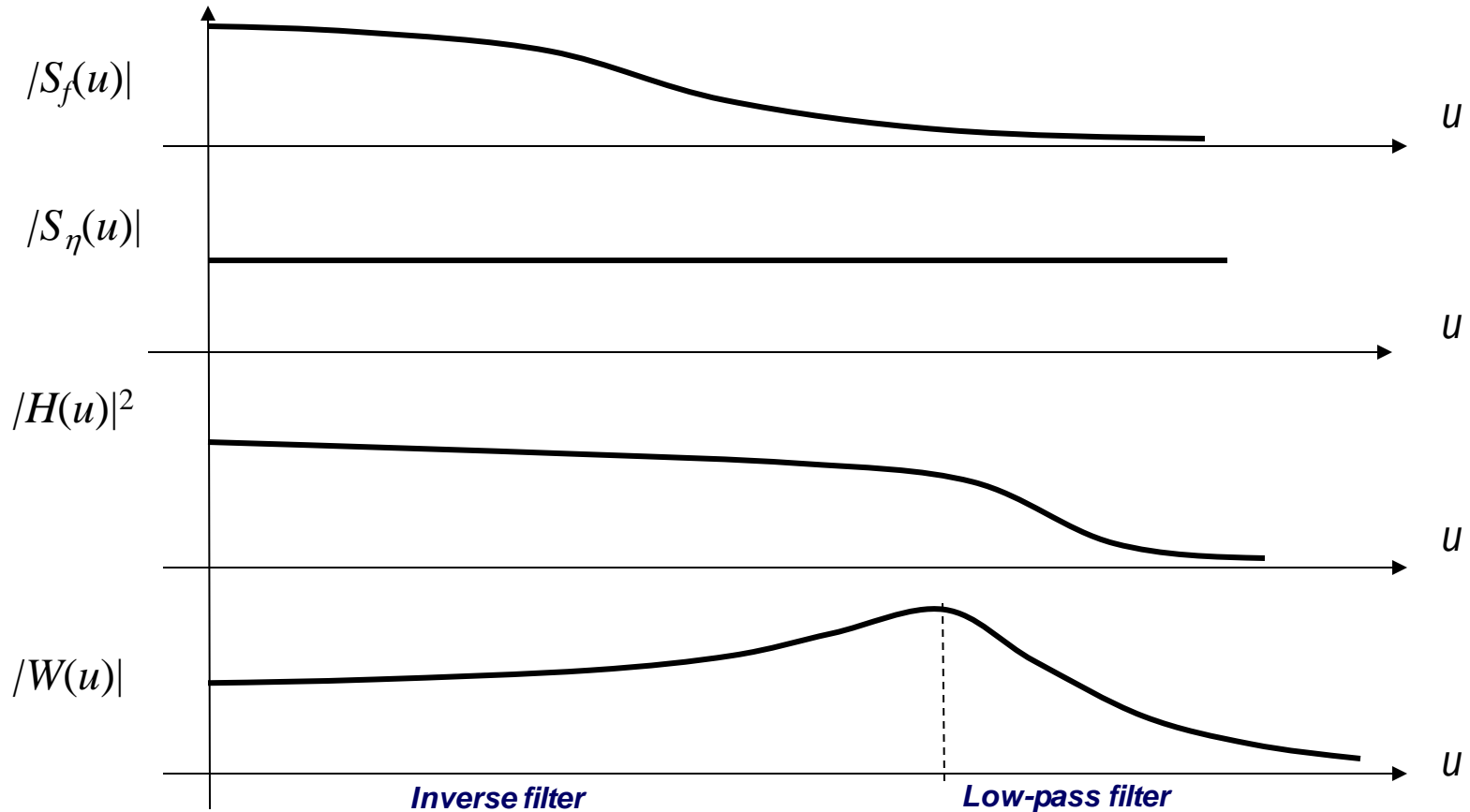
restauration by  
Wiener filtration

$L=31$   $\nearrow \varphi=45^\circ$





# Wiener filter





# Image restoration



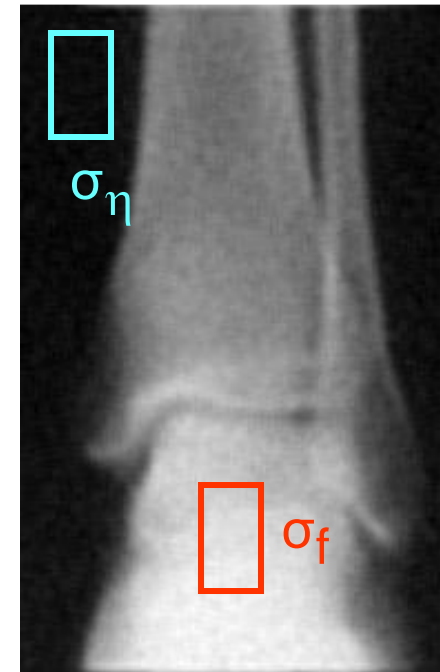
original image



degradation + noise



Wiener filter



simplified Wiener filter  
 $K = \sigma_{\eta} / \sigma_f$



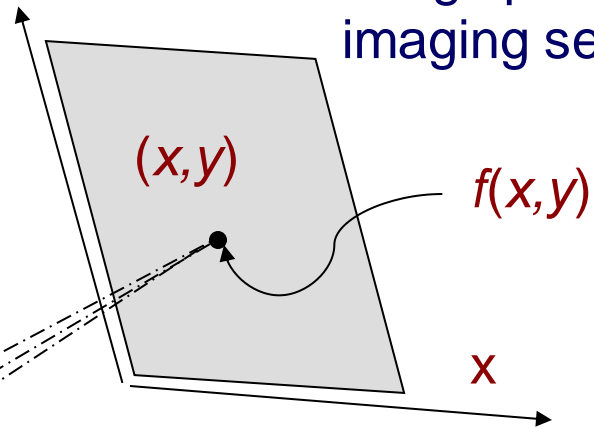


# Point Spread Function (PSF)

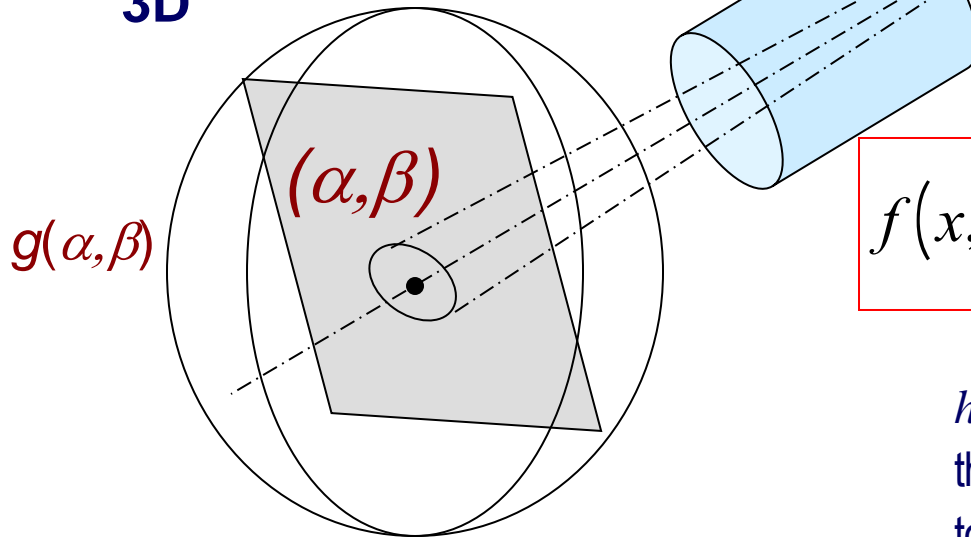
$$h(x, y) = \exp\left(-\frac{x^2 + y^2}{2\sigma^2}\right)$$

Image formation model

Image plane of the imaging sensor



3D



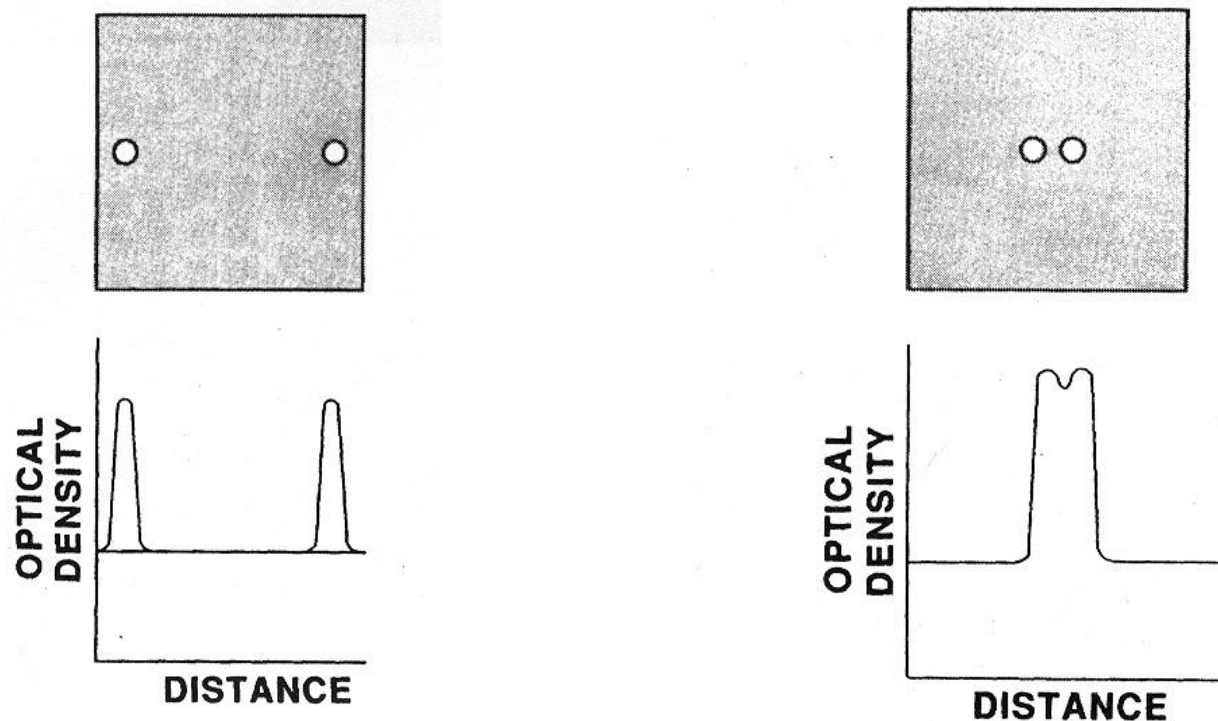
$$f(x, y) = \int_{-\infty}^{\infty} \int_{-\infty}^{\infty} g(a, b) h(x, y, a, b) da db$$

$h(\cdot)$  – is termed the **point spread function** of the imaging system; it describes its response to a point source.



# Point Spread Function (PSF)

PSF is a measure of a minimum distance between two objects when they can be clearly distinguished in the image



closer structures are interpreted as a single image objects – their boundaries overlap



# Modulation Transfer Function

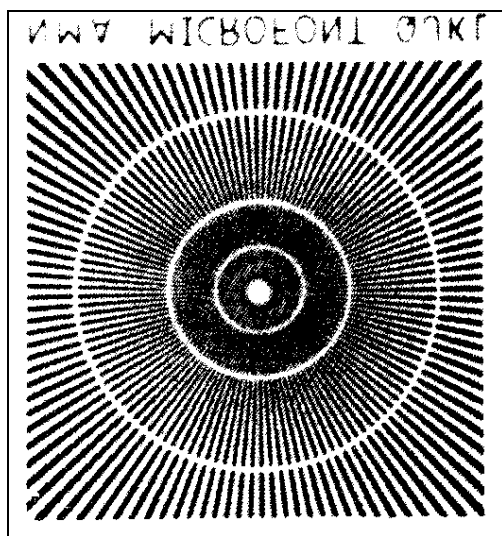
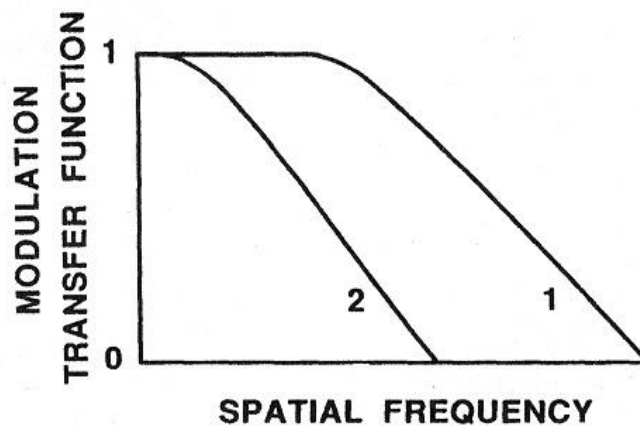
$$F(u, v) = G(u, v)H(u, v)$$

MTF is a Fourier transform of PSF. It represents a frequency characteristics of the imaging system.

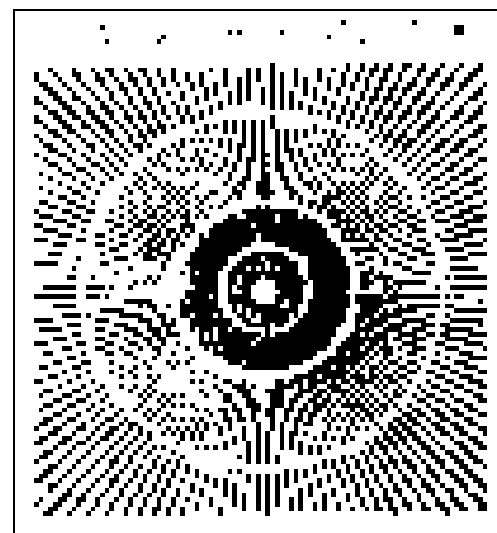
$$H(u, v) = \mathbf{F}[h(x, y)]$$



# Modulation Transfer Function

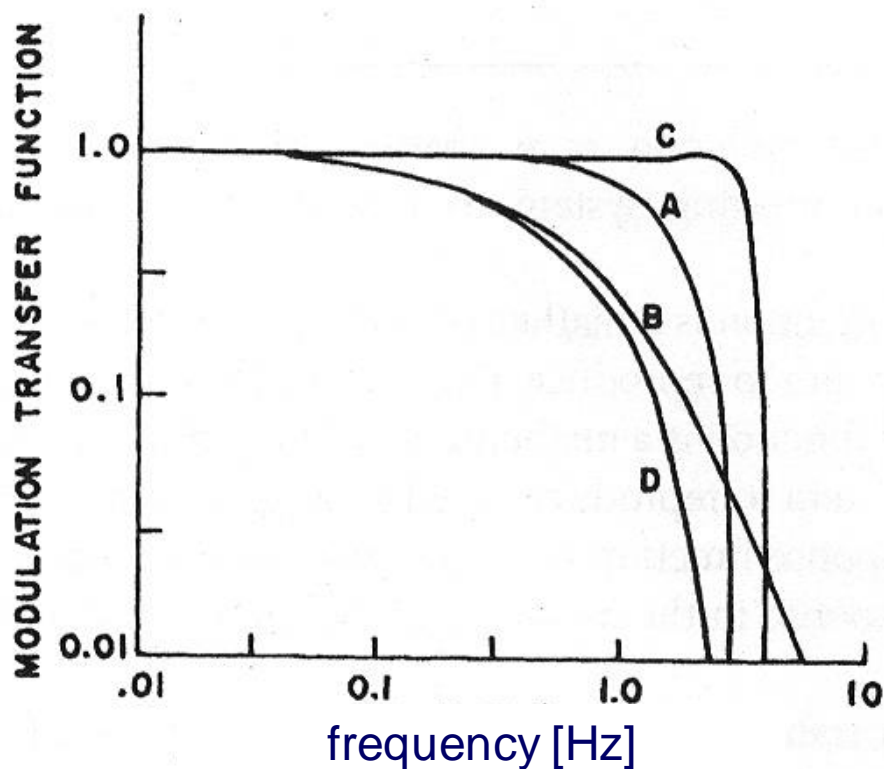


MTF 1  
500 dpi



MTF 2  
100 dpi

# Modulation Transfer Function



MTFs of radiographic imaging system:

- A) screen-film
- B) image formation system
- C) object motion
- D) resulting function for the entire system



## References

- W. R. Hendee, E.R. Ritenour, Medical Imaging Physics, Wiley-Liss, 2002
- C. Guy, D. ffytche, An Introduction to The Principles of Medical Imaging, Imperial College Press, 2008







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